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# Neuronavigation-Guided Focused Ultrasound-Induced Blood-Brain Barrier Opening: A Preliminary Study in Swine

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## ABSTRACT

**BACKGROUND AND PURPOSE:** FUS-induced BBB opening is a promising technique for noninvasive and local delivery of drugs into the brain. Here we propose the novel use of a neuronavigation system to guide the FUS-induced BBB opening procedure and investigate its feasibility in vivo in large animals.

**MATERIALS AND METHODS:** We developed an interface between the neuronavigator and FUS to allow guidance of the focal energy produced by the FUS transducer. The system was tested in 29 swine by more than 40 sonication procedures and evaluated by MR imaging. Gd-DTPA concentration was quantitated in vivo by MR imaging R1 relaxometry and compared with ICP-OES assay. Brain histology after FUS exposure was investigated using H&E and TUNEL staining.

**RESULTS:** Neuronavigation could successfully guide the focal beam, with precision comparable to neurosurgical stereotactic procedures ( $2.3 \pm 0.9$  mm). A FUS pressure of 0.43 MPa resulted in consistent BBB opening. Neuronavigation-guided BBB opening increased Gd-DTPA deposition by up to 1.83 mmol/L (a 140% increase). MR relaxometry demonstrated high correlation with ICP-OES measurements ( $r^2 = 0.822$ ), suggesting that Gd-DTPA deposition can be directly measured by imaging.

**CONCLUSIONS:** Neuronavigation provides sufficient precision for guiding FUS to temporally and locally open the BBB. Gd-DTPA deposition in the brain can be quantified by MR relaxometry, providing a potential tool for the in vivo quantification of therapeutic agents in CNS disease treatment.

**ABBREVIATIONS:** CE = contrast-enhanced; FUS = focused sonography; Gd-DTPA = gadolinium-diethylene-triamine pentaacetic acid; ICP-OES = inductively coupled plasma optical emission spectroscopy; MRgFUS = MR-guided FUS; SI = signal intensity; TUNEL = terminal deoxynucleotidyl transferase biotin-dUTP nick end-labeling

The BBB prevents molecules larger than 400 Da from entering the brain parenchyma, protecting it from toxic foreign substances and preventing entry of therapeutic drugs.<sup>1,2</sup> The perme-

ability of the BBB can be increased by FUS using microbubbles and a low-energy burst tone.<sup>3,4</sup> This noninvasive procedure disrupts the BBB locally, rather than systemically, to minimize off-target effects, and disruption is reversible within several hours. BBB opening can be confirmed by increased permeability of MR imaging contrast agents such as Gd-DTPA<sup>3-5</sup> or superparamagnetic iron oxide nanoparticles.<sup>6</sup>

Sonography focal energy needs to be guided with high precision to open the BBB at a specific target. One successful approach is MRgFUS, originally designed for monitoring and guiding thermal ablation by an embedded FUS system inside the MR bore. Brain tissues have been successfully ablated transcranially by monitoring the temperature response in both large animals<sup>7</sup> and humans<sup>8,9</sup>; however, widespread use of MRgFUS is hampered by its design complexity and cost. In addition, MR scanners block access of neurosurgeons to patients, and most surgical tools were not designed to be MR compatible. Although the focal beam can be localized by the slight temperature elevation caused by weak, continuous wave exposure, actual BBB opening can currently

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only be confirmed by MR contrast agent leakage after, but not during, the sonication process.<sup>3,10</sup> Thus, despite the successful demonstration of FUS BBB opening in large animals, MR imaging has only served as a postoperative verification tool and has not addressed the issue of guidance of FUS energy during the procedure.<sup>11-13</sup> An alternative approach is therefore needed to integrate FUS as one of an array of available neurosurgical tools while preserving the excellent capability of precise focal beam guidance of the MRgFUS system.

The neuronavigational guidance system has revolutionized neurosurgery by providing a way to navigate through the body using 3D images.<sup>14</sup> Preoperative diagnostic scans of patients (usually CT images or MR imaging) are first analyzed, followed by a registration process that allows 3D localization of the surgical tools and that assists neurosurgeons in mapping the safest, least invasive path to the target site for tumor removal surgery, interstitial interventions, or biopsy. Currently, however, only standard solid surgical instruments, such as biopsy needles, catheters, or microsurgical robots, can be guided, as neuronavigation of the focal energy generated by a FUS transducer in CNS tissues has not been attempted.

The purpose of our study was to design a procedure for neuronavigation-guided FUS brain drug delivery by guiding the focal beam and to investigate its feasibility in vivo in large animals (swine, *Sus scrofa domestica*).

## MATERIALS AND METHODS

### Neuronavigation Guidance Setup

We used a neuronavigation system (Stryker, Freiburg, Germany) to guide FUS BBB opening. The procedure was initiated by registering the focal point of the FUS transducer on the neuronavigation system. A sonography-permeable balloon-type membrane was then tightly fitted to the sonography transducer to fully cover the active elements and couple the sonography energy from the transducer element to the animal brain (the detailed procedure is provided in On-line Fig 1).

### Focused Sonography Exposure

Animals were anesthetized by isoflurane. The top of the cranium was shaved and a PE-50 catheter (Instech Labs, Plymouth Meeting, Pennsylvania) was inserted into the ear vein for injections. During FUS treatment, sonography microbubbles were constantly infused through the ear vein (SonoVue; Bracco Diagnostic, Milan, Italy) at 0.3 mL/kg/min. Sonography was delivered transcranially by a spherical single-element transducer (Imasonics, Besancon, France; diameter = 60 mm, radius of curvature = 80 mm, frequency = 400 kHz; measured half-maximum pressure amplitude diameter approximately 4 mm; length of the produced focal spot approximately 23 mm). Animal experiments were divided into 4 groups (On-line Table 1). In groups 1, 2, and 3 ( $n = 5, 9$ , and  $9$ , respectively), we evaluated the accuracy of neuronavigation-guided BBB opening with different negative peak pressures (0.26, 0.43, and 0.56 MPa, respectively, after considering skull and tissue decay) using a single FUS exposure. This experiment also allowed us to determine the BBB-opening threshold pressure. FUS energy was delivered in burst-tone mode, with burst length = 10 ms, pulse-repetition frequency = 1 Hz, and

sonication duration = 30 seconds. In group 4 ( $n = 6$ ), we investigated whether we could also obtain large BBB-opened regions with expected target volumes by precise neuronavigational guidance of multipoint FUS exposures ( $3 \times 3$  arrangement, 5-mm spacing; 0.43-MPa sonication). All animals were humanely killed within 24 hours.

Calibrated ultrasonic pressure and focal beam dimensions were measured both with and without a harvested swine skull, and the pressure loss caused by skull distortion was estimated to be 30%, with no apparent focal beam shift (On-line Fig 1C, -D). Transcranial pressure loss measured in the human skull was approximately 40% (data not shown).

### MR Imaging

MR imaging was conducted with a 3T MR imaging scanner (Trio with Tim; Siemens, Erlangen, Germany). All animals underwent an initial MR imaging scan for setup, registration, and treatment planning for the neuronavigation system, and another scan to evaluate the treatment outcome. Animals were placed in a homemade stereotactic frame mounted on a position-fixed deck to guarantee identical imaging orientations for MR imaging scans.

Animals were anesthetized by intraperitoneal injection of chlorohydrate (30 mg/kg). Gd-DTPA (0.1 mmol/kg; Magnevist; Berlex Laboratories, Wayne, New Jersey) was administered, followed by saline (0.2 mL/kg) and heparin (0.2 mL/kg). T1-weighted MR images were acquired immediately after the completion of Gd-DTPA administration (TR/TE = 700 ms/11 ms), followed by acquisition of T2-weighted images (TR/TE = 3260 ms/96 ms).

A heavy T2\*-weighted fast low-angle shot sequence with full flow compensation in all 3 directions (TR/TE/flip angle = 28 ms/20 ms/15°) was modified to produce SWI for identifying intracerebral hemorrhaging caused by excessive FUS exposure.<sup>15</sup>

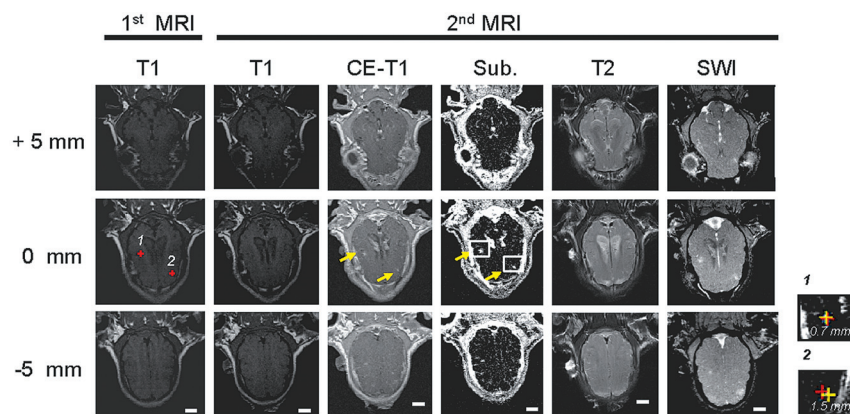
R1 relaxivity was quantified by transferring signal intensities from 2 T1-weighted gradient recalled-echo images with different flip angles, as previously described (TR/TE = 101 ms/4.1 ms, flip angle = 20°/40°).<sup>16,17</sup> In vitro phantom measurements showed that the R1 relaxation rate was linearly proportional to Gd-DTPA concentration (On-line Fig 2). These measurements were used to calibrate the R1 relaxivity rate (in seconds<sup>-1</sup>) and estimate R1 relaxivity (3.821 mmol/L<sup>-1</sup> second<sup>-1</sup>). Identical MR imaging sequence setups were then applied to the animal MR imaging scans. We also quantitated Gd-DTPA deposition in the BBB-opened brain by ICP-OES assays and compared our findings with R1 relaxometry (see On-line materials).

### Evaluation of Accuracy of Neuronavigation Guidance

The accuracy of neuronavigation in guiding FUS BBB opening was quantified by measuring the discrepancy between the assigned and actual BBB opening location on the focal plane.

### Histologic Examination

Evans blue dye was administered after MR imaging for gross observation of the BBB-disrupted region. Animals were sacrificed and brain tissue samples from the sonicated sites and contralateral (control) hemispheres were fixed in formaldehyde. In each animal, 5–20 frozen sections (10- $\mu$ m thick) covering the FUS exposure regions were stained by hematoxylin and eosin to assess hemorrhagic dam-



**FIG 1.** Typical MR image sets (0.43-MPa pressure). Column 1: T1-weighted images obtained in the first MR imaging scan (before FUS exposure, for neuronavigation guidance). Columns 2–4: T1, CE-T1, and subtracted T1-weighted images obtained in the second MR imaging scan (after FUS exposure, for treatment validation). Column 5: T2-weighted images. Column 6: Susceptibility-weighted images. Zoomed regions (*right*) demonstrate the measured discrepancy between the targeted and maximum SI increase locations at targets 1 and 2 (0.7 and 1.5 mm, respectively).

age. Another 3–6 sections were stained by TUNEL assay (ApopTag kit; Intergen, New York, New York). Histologically confirmed tissue damage was characterized by various grades of increasing damage.<sup>15,18</sup>

## RESULTS

A typical MR imaging result is shown in Fig 1. The identical image orientation of the first and second T1 scans (Fig 1, columns 1 and 2) suggested minimal animal movement in the stereotactic holder. The positions of 2 selected FUS exposure locations (yellow markers) were entered into the neuronavigation system for focal-beam guidance. The BBB-opened regions were clearly visible in the T1, CE-T1, and subtracted images (Fig 1, columns 2–4) of the second scan but quickly disappeared when leaving the focal depth, suggesting that they were close to the planned depth of treatment. The discrepancies between the BBB-opened regions and the planned target points 1 and 2 were 0.7 and 1.5 mm, respectively, in the coronal focal plane (Fig 1, zoomed images), indicating that neuronavigation successfully guided the focal beam to the targets. The unchanged T2-weighted images (Fig 1, column 5) showed that there was no brain edema for this treatment exposure. Moreover, the lack of signal decay in the T2\* image (Fig 1, column 6) indicated that the intracerebral hemorrhage had not occurred during sonication. The slight signal increase at the BBB-opened regions was probably caused by Gd-DTPA leakage.

We compared the R1 map results of the brain before and after FUS exposure and Gd-DTPA injection (Fig 2A). The BBB-opened regions showed a high R1 relaxation rate ( $>4 \text{ seconds}^{-1}$  compared with  $<2 \text{ seconds}^{-1}$  in the contralateral brain). From the Gd-DTPA relaxivity, we estimated that Gd-DTPA was deposited at a concentration of more than 1.05 mmol/L in the BBB-opened region, compared with less than 0.52 mmol/L in the contralateral brain. FUS exposure thus enabled leakage of at least 0.5 mmol/L Gd-DTPA into brain parenchyma. These contrast enhancement areas were supported by the distribution of Evans blue dye in comparable brain sections (Fig 2B).

The mean distance discrepancy between the target point and

the BBB-opened location for all experiments (0.43-MPa and 0.56-MPa exposures) was  $2.3 \pm 0.9 \text{ mm}$  (Fig 3A), which is within the acceptable range of clinical neuronavigational guidance.

We investigated the effect of different pressure levels on BBB opening (Fig 3B). Gd-DTPA contrast enhancement suggested consistent BBB opening at a pressure of 0.43 MPa (SI increase =  $17.9 \pm 11.6\%$ ) but not at 0.26 MPa (SI increase =  $-0.3 \pm 10.9\%$ ). Further increasing the FUS pressure to 0.56 MPa provided higher contrast enhancement (SI =  $28.1 \pm 23.8\%$ ). We also measured the change of relaxation rate caused by BBB opening. An exposure of 0.26 MPa failed to produce any apparent change in the R1 relaxivity rate ( $-0.15 \pm 0.45 \text{ seconds}^{-1}$ ), whereas higher pressure levels of 0.43 or

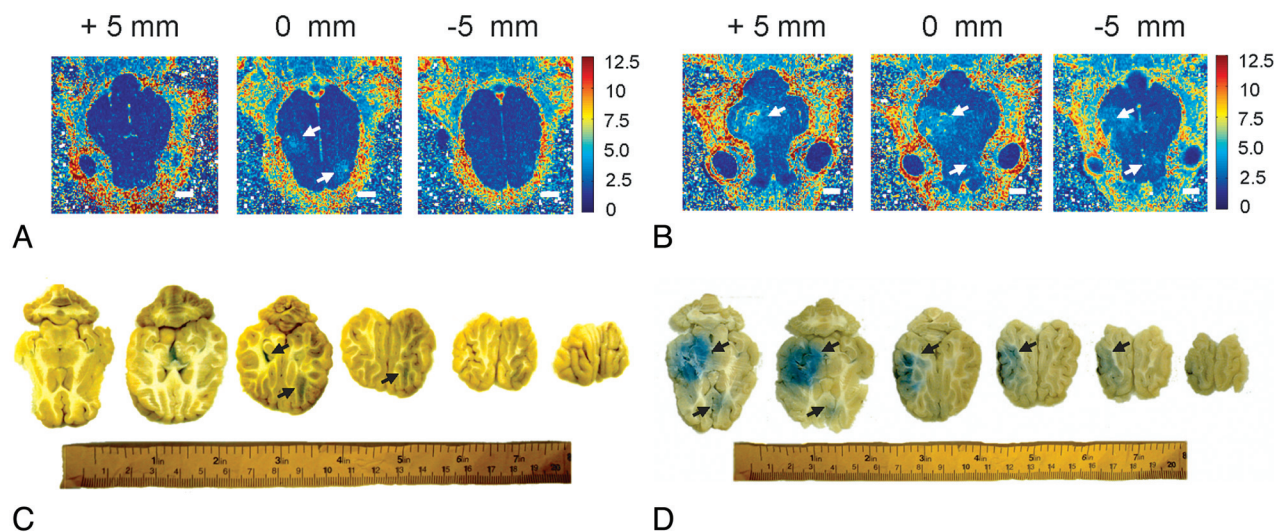
0.56 MPa produced significant monotonic increases in relaxivity rates— $1.15 \pm 0.95 \text{ seconds}^{-1}$  ( $26.6 \pm 19.9\%$  to contralateral brain) and  $2.45 \pm 1.65 \text{ seconds}^{-1}$  ( $79.0 \pm 36.9\%$  to contralateral brain), respectively (Fig 3C)—equivalent to 0.3 and 0.6 mmol/L of Gd-DTPA permeating into brain parenchyma. Thus, neuro-navigation could provide sufficient precision in guiding FUS to temporally and locally open the blood-brain barrier, and Gd-DTPA deposition of up to 1.83 mmol/L (140% increase) could be achieved by 0.56 MPa sonication.

We measured the correlation between Gd-DTPA contrast-enhanced signal changes in MR imaging, and Gd-DTPA concentrations measured by ICP-OES assay, for 36 tissue samples obtained from 2 animals (Fig 3E). The T1 contrast-enhanced change was well correlated with the measured gadolinium concentration ( $r^2 = 0.598$ ) and could therefore provide semiquantitative information on gadolinium deposition in the BBB-opened brain. However, R1 maps were found to provide direct *in vivo* quantification of the amount of Gd-DTPA leaked into the BBB-opened region and also showed improved correlation with the measured concentrations (Fig 3F;  $r^2 = 0.822$ ).

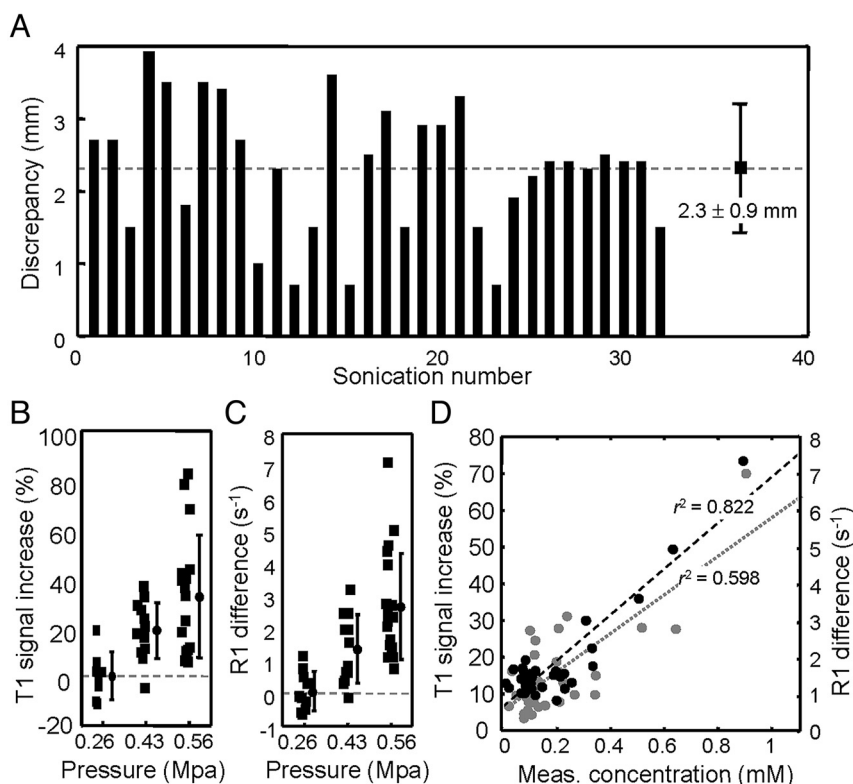
Next we showed that a large BBB-opened region could be successfully created by multipoint FUS exposure performed in a  $3 \times 3$  shape, with 5-mm spacing between each sonication point (Fig 2C; group 4 animals). The diameter of the opening was significantly enlarged (approximately 20 mm) in the coronal plane compared with single-point sonication (4 mm). A brain section of the same animal confirmed significant enlargement of BBB opening (Fig 2D).

Tissues from regions exposed to FUS at different levels of pressure were histologically classified (On-line Fig 3). The 0.26-MPa exposure did not consistently introduce a BBB-opening effect and a most of the samples were unchanged upon H&E staining. Some samples had vasodilations. Tissues from the 0.43-MPa exposure were also mostly intact, with occasional nongrouping erythrocyte extravasations (8.6%). Grouping extravasations increased by 3.1% for 0.56-MPa exposure, and further increased to 6.4% in multiple 0.43-MPa sonication exposures. Nevertheless, none of these perivascular hemorrhage locations showed signal changes in





**FIG 2.** RI maps and the Evans blue-stained brain sections obtained from single-point (A, B; same animal as Fig 1) and multipoint ( $3 \times 3$ ) FUS exposures (C, D). Arrows denote significant RI (A, B) or Gd-DTPA leakage regions (C, D). Size bar = 10 mm.



**FIG 3.** A, Discrepancy (in mm) between the planned target point and BBB-opening points measured from subtracted CE-T1-weighted images of all experiments. The average discrepancy was  $2.3 \pm 0.9$  mm. B, MR imaging signal intensity increase obtained from the signal differences between T1- and CE-T1-weighted images at the sonication target after different FUS exposure levels (0.26, 0.43, and 0.56 MPa). C, The difference (in seconds<sup>-1</sup>) between RI measurements of the first and the second (postoperative) MR imaging scans under different FUS pressures (0.26, 0.43, and 0.56 MPa). D, Correlation between the measured Gd concentration (in mM; from ICP-OES assay; gray marker) and the SI contrast enhancement (in %) obtained from T1 images, and correlation between the measured Gd concentration (in mM) from ICP-OES assay and the estimated Gd concentration (in mM) from MR imaging RI maps (black markers).

slides), a total of 9.5% appeared erythrocyte extravasations but still within a controlled and secure scale,<sup>3,18</sup> and a low incidence (2.3%) of unacceptable microhemorrhage level was identified only from group 3 and 4 experiments. All TUNEL staining was negative, suggesting that FUS did not cause apoptosis (On-line Table 2). This implies that it is possible to choose FUS exposure conditions that will securely open the BBB in large animals.

## DISCUSSION

Here we demonstrated the successful use of a neuronavigation system to guide FUS-induced BBB opening. The threshold pressure level required for BBB opening in swine was similar to that reported in mice<sup>5,19</sup> and primates.<sup>11</sup> Compared with the MR-guided approach, neuronavigation allows monitoring of BBB opening during the FUS process and significantly reduces costs. A one-time-only MR imaging procedure is sufficient for guidance, which is particularly important for patients undergoing multiple chemotherapeutic treatments, such as brain cancer patients. Neuronavigation has the added advantage of not limiting neurosurgical intervention by MR imaging chamber space or nonmagnetic properties, thus providing high treatment flexibility.

The positional discrepancy of our method (2.3 mm) was similar to the currently accepted value of neuronavigational surgical-tool guidance (approximately 2 mm).<sup>14,20</sup> Positional errors are known to arise from several sources,<sup>14</sup> but the most probable source in our study

the T2\* images, indicating that perivascular hemorrhaging remained below the limit of MR imaging detection. Among the 29 animals conducted histological examinations (with 1720 H&E

is fiducial facial attachment during registration. This could be improved by a skull-implant fiducial, but the process is invasive. Another source of error comes from sonography being diffracted by inhomogeneous bone. The accuracy could likely be increased by the addition of phase correction to a phased array system using CT.

Postoperation MR R1 relaxometry was used to evaluate the success of FUS-induced BBB opening. We found that the Gd-DTPA concentration was linearly proportional to the R1 relaxation rate. Compared with the qualitative confirmation of BBB opening obtained from contrast-enhanced T1 images, relaxometry provided a direct and better measurement of Gd-DTPA. Previous small-animal studies have demonstrated that the Gd-DTPA concentration determined from the MR imaging SI change is well correlated with the delivered drug concentration,<sup>21,22</sup> and our findings revealed the potential of R1 relaxometry to further improve the accuracy and reliability of semiquantitative estimation of local CNS drug delivery.

Tumors are usually bulky (typically 50–90 mL in volume) and have highly heterogeneous blood-tissue permeability.<sup>23,24</sup> Large openings in the BBB are therefore desirable for brain tumor treatment in order to affect as many brain tumor cells as possible, including diffusely scattered tumor cells that are often found outside the main contrast enhancement area, adjacent to the FUS BBB-opening site.<sup>25</sup> We found that FUS exposure in a  $3 \times 3$  pattern successfully created a large BBB-opening region (>20 mm) compared with a single FUS exposure (<5 mm). However, the efficacy of BBB opening is highly dependent on the temporal concentration of microbubbles in the bloodstream.<sup>26</sup> We therefore controlled the microbubble infusion rate to maintain a constant circulatory bubble concentration during exposure. With a maximum allowable microbubble volume, the overall exposure time has to be limited. A future improvement would be to use a sonography-phased array capable of fast scanning of the focus position via switching the phase difference among elements, thus significantly increasing the total number of FUS exposures.

## CONCLUSIONS

Our successful demonstration of neuronavigation-guided FUS in the swine brain has the potential to become a widely used and flexible medical tool for drug delivery across the BBB into the human brain. The proposed concept could be easily integrated with current neurosurgical interventions. In addition, the design complexity of the FUS system could be reduced by combination with neuronavigation systems already in widespread use, lowering the cost of the overall system. Neuronavigation-guided FUS reduces the requirement of the entire device on MR compatibility and could be used in combination with other anatomic imaging tools. Gd-DTPA relaxometry could be expanded to monitoring or quantifying future in vivo therapeutic agents through imaging, either through direct conjugation to Gd-DTPA or by extrapolation from its relative leakage efficiency compared with that of Gd-DTPA, keeping in mind the strong dependence of BBB permeability on size. The application of a neuronavigation system in guiding FUS for BBB opening will provide a new and more flexible route of accomplishing FUS-enhanced brain drug delivery

and is expected to speed up the translation process and widespread use of this technology.

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