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MR of Epidermoids with a Variety of Pulse Sequences

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PURPOSE: To assess the usefulness of fluid-attenuated inversion recovery (FLAIR) and constructive interference in steady state (CISS) sequences in depicting epidermoid tumors. **METHODS:** Six patients with surgically confirmed epidermoid tumors in the subarachnoid space were examined with T1-weighted MR imaging with a spin-echo sequence, and with T2- and proton density-weighted imaging with a fast spin-echo sequence, a FLAIR sequence, and a CISS sequence. In the qualitative analysis, three observers compared the five sequences for visibility of tumors and presence of artifacts. A quantitative analysis was also performed by measuring the contrast-to-noise ratio. **RESULTS:** On visual assessment, the FLAIR sequence depicted all tumors as hyperintense relative to cerebrospinal fluid. The CISS sequence depicted all tumors as hypointense relative to cerebrospinal fluid and was considered to show tumor extension better than the FLAIR sequence. At quantitative analysis, the mean contrast-to-noise ratios of tumor to cerebrospinal fluid on T1-, T2-, and proton density-weighted images, and on FLAIR and CISS sequences were 2.85, 3.41, 4.42, 16.13, and 20.23, respectively. The contrast-to-noise ratios for the FLAIR and CISS sequences were significantly higher than those for the T1-, T2-, and proton density-weighted sequences. The contrast-to-noise ratio was not significantly different between FLAIR and CISS sequences, although the CISS sequence was slightly superior. **CONCLUSION:** CISS and FLAIR sequences depicted epidermoid tumors in the subarachnoid spaces better than conventional spin-echo images did. The CISS sequence produced a relatively constant contrast between the tumors and less artifactual interference.

Index terms: Epidermoid; Brain neoplasms, magnetic resonance; Magnetic resonance, comparative studies

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Epidermoid tumors are congenital lesions of ectodermal origin, representing 0.2% to 1.8% of all primary intracranial tumors (1). They are usually found in the cerebellopontine angle, sellar and parasellar regions, and middle cranial fossa. At magnetic resonance (MR) imaging they are isointense to slightly hyperintense relative to cerebrospinal fluid (CSF) on T1-, T2-, and proton density-weighted images (1–6). It is

sometimes difficult to discern the exact extension of an epidermoid tumor using only T1-, T2-, or proton density-weighted imaging. Although diffusion-weighted imaging may show epidermoid tumors (7), it often produces unsatisfactory results because of patient movement and pulsatile brain movement. A steady-state free precession sequence with a short repetition time and a moderate flip angle is also useful for showing extension of epidermoid tumors (8). However, on this sequence, the demarcation between tumor and brain is poor, and it is sometimes difficult to find the repetition time and flip angle that provide the optimal contrast between tumor and CSF.

The fluid-attenuated inversion-recovery (FLAIR) sequence produces heavy T2 weighting without high signal intensity of CSF. The constructive interference in steady state (CISS) sequence can provide high-resolution images

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with good contrast between CSF and solid structures (9–11).

In this study, we used FLAIR and CISS sequences to evaluate epidermoid tumors. We compared the visibility of epidermoids on spin-echo T1-weighted images, fast spin-echo T2-weighted images, fast spin-echo proton density-weighted images, and FLAIR and CISS sequences.

Subjects and Methods

The study population consisted of six consecutive patients with untreated or residual epidermoid tumors: four female and two male, ranging in age from 11 to 71 years (mean, 53 years). The diameter of the tumors ranged from 1.5 to 6.5 cm. Three were located in the cerebellopontine angle cistern, two in the prepontine cistern, and one in the left middle fossa. Two were imaged before surgery and four were residual tumors imaged after surgery. The diagnosis and location of five of the six tumors were confirmed surgically.

All patients were imaged in a 1.5-T MR unit equipped with a head coil. For all patients, imaging examinations included axial T1-weighted spin-echo imaging (670/14/1 [repetition time/echo time/excitations]); axial T2-weighted fast spin-echo imaging (4500/96/2; echo train length, 7); axial imaging with a FLAIR sequence (8000/119/1; echo train length, 7; inversion time, 2000); and axial imaging with a CISS sequence (17.1/8.0/1; flip angle, 80°). Four of six patients also underwent proton density-weighted fast spin-echo imaging (2400/15/2; echo train length, 7). Other imaging parameters were as follows: matrix size was 256×256 for the T1-weighted, proton density-weighted, and FLAIR sequences and 512×256 for the T2-weighted sequences; section thickness was 5 mm with 1-mm intersection gaps for the T1- and T2-weighted and FLAIR sequences; and field of view was 220 mm. Imaging parameters for the CISS sequence were as follows: matrix size was 512×256 , section thickness was 0.71 mm (50-mm slab thickness for the 70 partitions), and field of view was 220 mm. The phase-encoding direction was right to left for all sequences.

For qualitative analysis, the depiction of tumor in the subarachnoid space was compared for the T1-, T2-, and proton density-weighted images, and the FLAIR and CISS sequences. These images were classified by three neuro-radiologists into four grades, as follows: 1, tumor not seen or only suspected on the basis of widening of the subarachnoid space; 2, tumor vaguely visible, but its exact extension not discernible; 3, extension of tumor partially unclear; and 4, tumor well demarcated. The readers were not blinded to the diagnosis or the pulse sequences.

Image artifacts on CISS and FLAIR sequences were also assessed qualitatively by the same interpreters, who judged image artifacts as follows: +1, fewer artifacts on CISS than on FLAIR sequences; 0, CISS and FLAIR sequences comparable; -1, fewer artifacts on FLAIR than on

CISS sequences. Each evaluator was also asked to indicate whether image artifacts interfered with the interpretation of the images. The following scale was used to evaluate the interference caused by artifacts: +1, artifacts caused interference on FLAIR sequences; -1, artifacts caused interference on CISS sequences. The statistical significance of differences in the qualitative analysis of image artifacts was determined by means of a sign test (12).

For the quantitative analysis, the contrast-to-noise ratio (CNR) between tumors and CSF was compared for T1-, T2-, and proton density-weighted images, and FLAIR and CISS sequences. The CNR was calculated as follows: $CNR = |\text{signal intensity of tumor} - \text{signal intensity of CSF}| / \text{standard deviation (SD) of noise}$. To minimize partial volume effects, we selected the image that showed the maximum area of the lesion and used a circular region of interest (ROI) that approached but did not exceed the lesion margins on the CISS sequences. The same ROI was selected on the spin-echo and FLAIR sequences. In the same image, CSF signal intensities were measured with the circular ROI chosen to be as large as possible to cover the CSF space. The SD of noise was measured along the phase-encoding direction in regions outside the head.

For statistical analysis, the data were analyzed using an unpaired *t* test.

Results

Qualitative Analysis

All epidermoids were isointense or nearly isointense with CSF on T1- and T2-weighted images, and isointense or slightly hyperintense on proton density-weighted images. Images obtained with these spin-echo sequences had low scores (grade 1 or 2) in all cases. Although the tumors were slightly to moderately hyperintense on FLAIR sequences, it was difficult to estimate their exact extension, especially for the postoperative small residual tumors. These cases were scored as grade 3 or 4 on FLAIR sequences. On the CISS sequence, all tumors were hypointense, and the demarcation between tumor and CSF was clear. All CISS sequences were scored as grade 3 or 4. Of the five sequences, CISS showed the tumors best (Figs 1–3). The interleaved CSF within the tumor was depicted only on the CISS sequence, and was confirmed at surgery (Fig 2). For overall image artifacts, CISS was rated inferior to FLAIR by two of three evaluators. However, when CISS and FLAIR sequences were compared for the prevalence of artifacts that could potentially interfere with image interpretation, CISS was rated superior to FLAIR by all three evaluators,

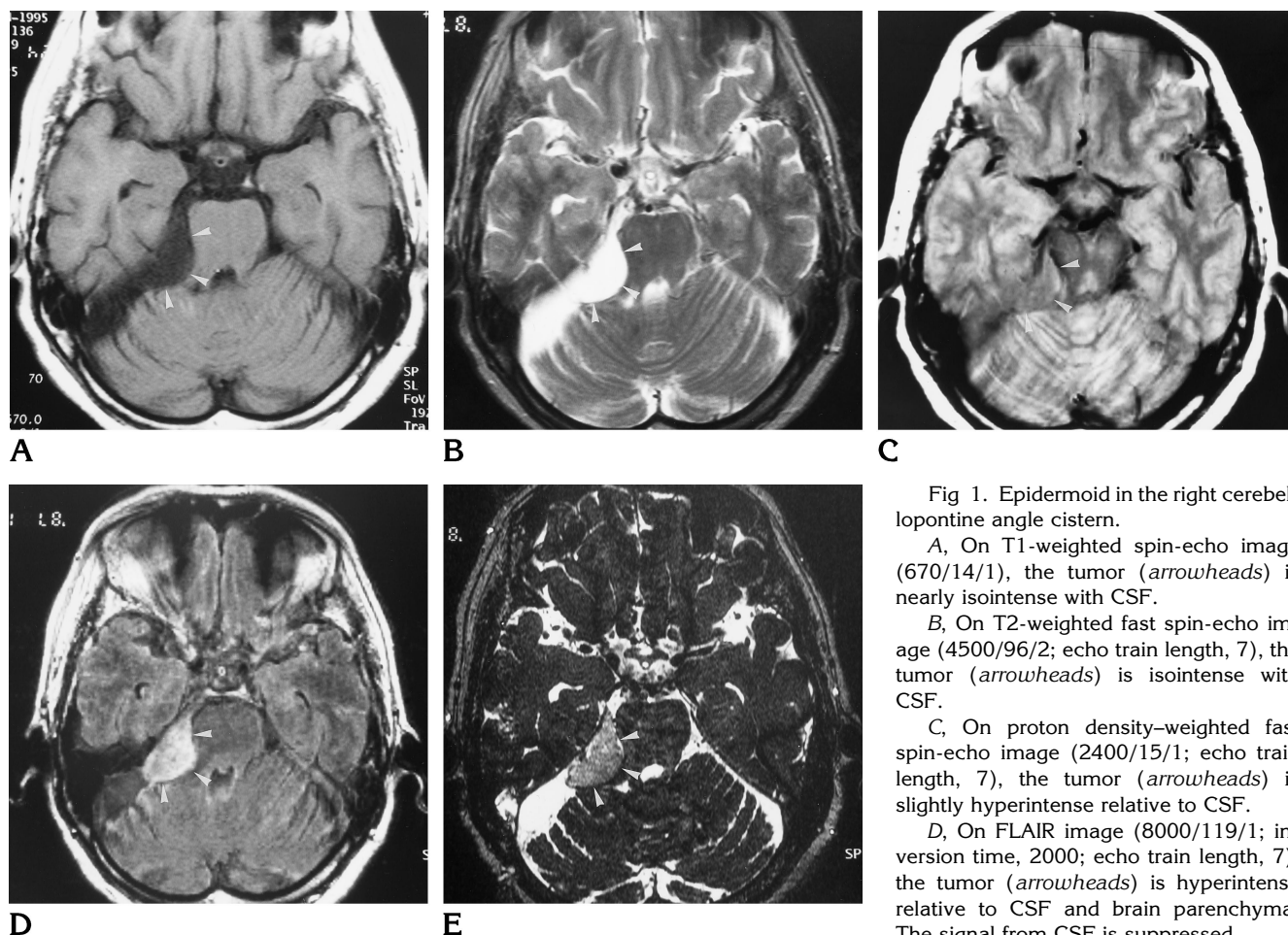


Fig 1. Epidermoid in the right cerebellopontine angle cistern.

A, On T1-weighted spin-echo image (670/14/1), the tumor (arrowheads) is nearly isointense with CSF.

B, On T2-weighted fast spin-echo image (4500/96/2; echo train length, 7), the tumor (arrowheads) is isointense with CSF.

C, On proton density-weighted fast spin-echo image (2400/15/1; echo train length, 7), the tumor (arrowheads) is slightly hyperintense relative to CSF.

D, On FLAIR image (8000/119/1; inversion time, 2000; echo train length, 7), the tumor (arrowheads) is hyperintense relative to CSF and brain parenchyma. The signal from CSF is suppressed.

E, On CISS image (17.1/8.0/1; flip angle, 80°), the tumor (arrowheads) is hypointense compared with CSF and hyperintense compared with brain parenchyma.

although the score was not statistically significant ($P < .05$).

Quantitative Analysis

The mean CNRs of tumors to CSF on T1-, T2-, and proton density-weighted images, and on FLAIR and CISS sequences were 2.85, 3.41, 4.42, 16.13, and 20.23, respectively. Ratios for FLAIR and CISS sequences were significantly higher than those for T1-, T2-, and proton density-weighted images ($P < .01$). Compared with FLAIR, CNR for CISS was higher in four cases, lower in one, and almost equal in one. The mean CNR between FLAIR and CISS sequences was not significantly different, although CISS was slightly better than FLAIR.

Discussion

Although epidermoid tumors typically are depicted by MR imaging as slightly hyperintense

relative to CSF on T1-, T2-, and proton density-weighted spin-echo sequences (1–6), the difference between these signals is small and it is frequently difficult to differentiate the tumors from arachnoid cysts on conventional spin-echo sequences (1–3, 5, 7, 8).

FLAIR is an inversion-recovery sequence designed to null or greatly reduce the signal from CSF; it gives heavy T2 weighting without high signal and potential artifacts from CSF (13). FLAIR images, however, show CSF flow artifacts, attributable to inflow of noninverted CSF, especially at the foramen of Monro, basal cisterns, and fourth ventricle (13). FLAIR has been reported to be more sensitive than conventional T1- and T2-weighted imaging in the detection of a wide range of diseases, such as multiple sclerosis, infarction, herpes simplex encephalitis, sarcoidosis, tuberous sclerosis, and intracranial tumors (9, 13–19). We know of one case report describing the use of FLAIR in which an

Fig 2. Epidermoid in the left middle fossa.

A, On FLAIR image (8000/119/1; inversion time, 2000; echo train length, 7), the tumor (*arrowheads*) is slightly hyperintense relative to CSF and hypointense relative to brain parenchyma.

B, On CISS image (17.1/8.0/1; flip angle, 80°), the tumor (*arrowheads*) is hypointense compared with CSF and hyperintense compared with brain parenchyma. The relationship between the epidermoid and the interleaved CSF is clearly demonstrated. The interleaved CSF could not be detected with any other sequence.

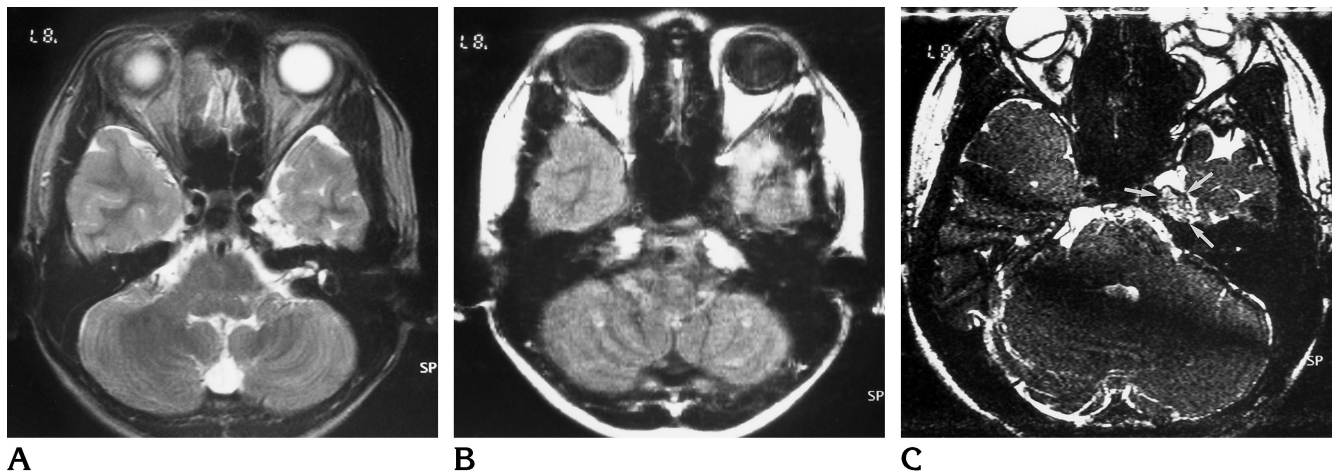
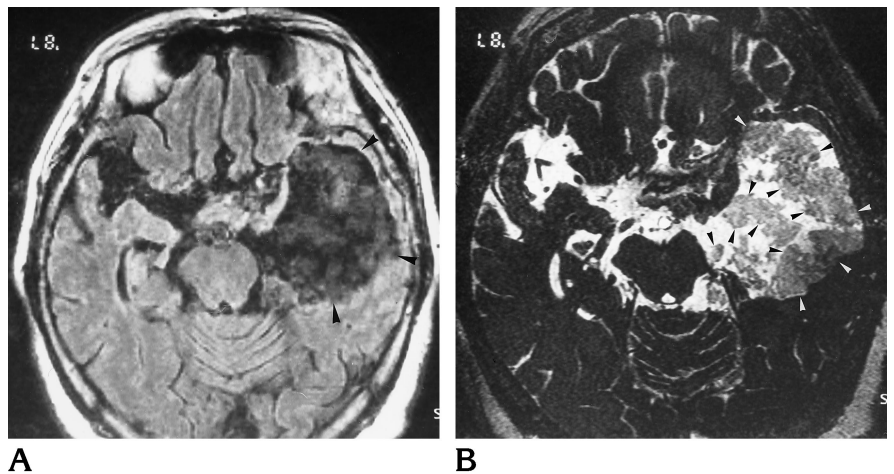


Fig 3. Postoperative residual epidermoid in left Meckel's cave.

A, On T2-weighted fast spin-echo image (4500/96/2; echo train length, 7), the tumor is not clearly detected. Meckel's cave is expanded on the left.

B, The tumor cannot be detected on FLAIR image (8000/119/1; inversion time, 2000; echo train length, 7).

C, On CISS image (17.1/8.0/1; flip angle, 80°), the tumor (*arrows*) is hypointense relative to CSF and is observed in the dilated left Meckel's cave.

epidermoid tumor appeared hyperintense relative to CSF (9). In that case, FLAIR was superior to conventional spin-echo sequences in depicting the tumor. In our study, the FLAIR sequence also depicted epidermoid tumors as hyperintense against the nulled signal from CSF. However, the CNR of the tumor in one case was very high, while in other cases it was very low. This variation in the CNR may have been due to a difference in hydration of the tumors. It is supposed that whereas dehydrated tumors have very high signal intensity on FLAIR sequences, the signal from tumors rich in water is suppressed by FLAIR, and they are poorly visualized. Moreover, on the FLAIR sequence, marked CSF flow artifacts attributable to the inflow of

noninverted CSF were often observed in the basal cisterns and prepontine or cerebellopontine angle cisterns, making it difficult to detect small lesions in these areas.

The CISS sequence was originally designed for MR myelography and MR cisternography. It is a true fast imaging with steady-state precision (FISP) sequence, which produces heavily T2-weighted images. However, a true FISP sequence will produce artifacts of low signal intensity bands. These dark bands are caused by very small magnetic-field inhomogeneities and local field distortions attributable to susceptibility changes that are normally produced in clinical imaging. CISS is an effective method of reducing these dark bands by the summation of

two three-dimensional Fourier transform (3DFT) data sets, one with an alternating radio frequency pulse and one with a nonalternating radio frequency pulse (10, 20) (M. Deimling, G. A. Laub, "Constructive Interference in Steady State for Motion Sensitivity Reduction," In: *Book of Abstracts: Society of Magnetic Resonance in Medicine*, 1989:842), and produces an image with a homogeneous intensity over the entire field of view and very high contrast between CSF and solid structures. The 3-D CISS sequence also provides high-resolution images with good contrast between CSF and solid structures. Several investigators have used the CISS sequence to demonstrate the fine anatomic structures of the inner ear or cerebellopontine angle (10, 11, 21). In our study, all epidermoid tumors were hypointense relative to CSF on CISS images. This contrast may have been due to the accentuation of T2 values between epidermoids and CSF, whereas in the T2-weighted images, an echo time of 96 milliseconds was not long enough to emphasize the difference in T2 values between them. Moreover, an epidermoid tumor is filled with cholesterol crystals and keratin originating from the progressive desquamation of the epithelium. It is supposed that these substances, which have differing susceptibilities, may decrease the signal of the tumor on CISS images. Although the CISS images did show susceptibility artifacts, these artifacts did not interfere with the detection of tumors. Because 3-D CISS sequences provided high spatial resolution with very thin sections, it was possible to detect the exact tumor extension, even for a small lesion in Meckel's cave (Fig 3). The variability observed on the CISS sequence was small compared with that of the FLAIR sequence. It is supposed that this variability on the CISS sequence was due to different proportions of substances contained in the epidermoids.

In conclusion, the FLAIR sequence depicted epidermoids with variable contrast. The CISS sequence produced relatively constant contrast and fewer artifacts interfering with interpretation than did FLAIR. Of the five sequences we evaluated, CISS was superior in demonstrating the exact extension of epidermoids.

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